

# On the Reproducibility of Deep Convolutional Neural Networks Approaches

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# Reproducibility issues in Deep Learning

## NVIDIA CUDA Deep Neural Network (cuDNN) Developer Guide

### 2.5. Reproducibility (determinism)

By design, most of cuDNN's routines from a given version generate the same bit-wise results across runs when executed on GPUs with the same architecture and the same number of SMs. However, bit-wise reproducibility is not guaranteed across versions, as the implementation of a given routine may change. With the current release, the following routines do not guarantee reproducibility because they use atomic operations:

- `cudaConvolutionBackwardFilter` when `CUDNN_CONVOLUTION_BWD_FILTER_ALGO_0` or `CUDNN_CONVOLUTION_BWD_FILTER_ALGO_3` is used
- `cudaConvolutionBackwardData` when `CUDNN_CONVOLUTION_BWD_DATA_ALGO_0` is used
- `cudaPoolingBackward` when `CUDNN_POOLING_MAX` is used
- `cudaSpatialTfSamplerBackward`

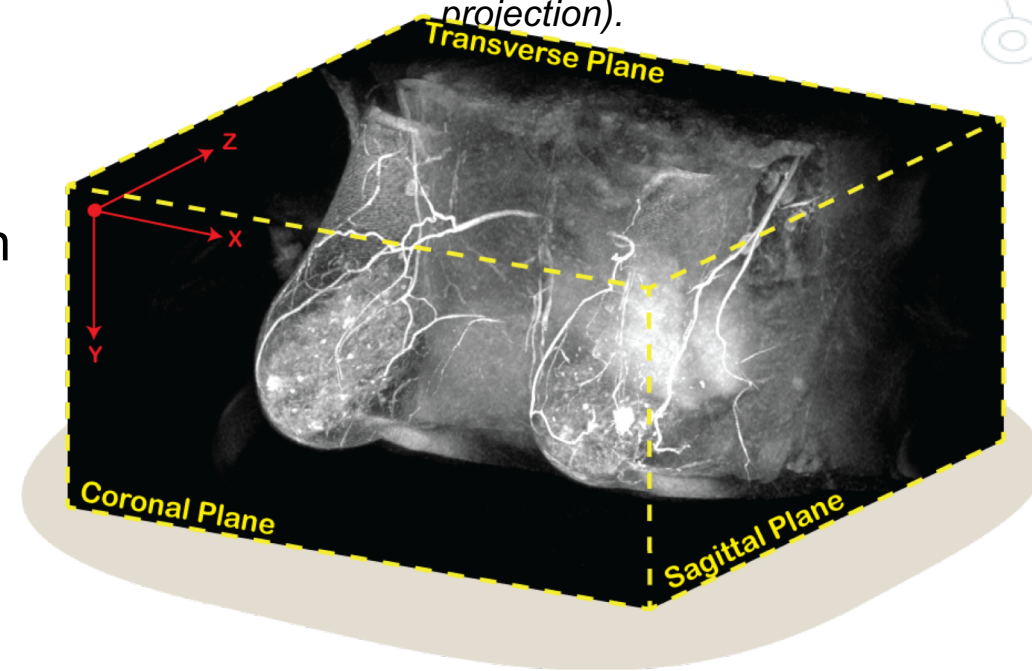
**Intuition:** the reproducibility issue can be shifted from a strictly combinatorial problem to a statistical one, in order to validate the model robustness and stability more than its perfect outcomes predictability

# Case Study: U-NET for Breast Tissues Segmentation

## Dynamic Contrast Enhanced-Magnetic Resonance Imaging (DCE-MRI)

- ✓ Important complementary diagnostic methodology
- ✓ Minimal invasiveness (non-ionizing radiation)
- ✓ Produces 4D volumes (3 spatial + 1 temporal)
- ✓ The paramagnetic contrast agent enhance vascularization
- ✓ Suited for under-forty patients
- ✗ Huge amount of data
- ✗ Long acquisition time.
- ✗ Involuntary patient movements

A 3D MRI volume [UP] (pre-contrast volume in maximum intensity projection).



# Case Study: U-NET for Breast Tissues Segmentation

Computer Aided Detection and Diagnosis systems (CAD)<sup>[1]</sup>



- **Volume Extraction**

The whole 4D volume (3 Spatial + 1 Temporal) is created from the DCE-MRI data.

- **BreastMask Extraction<sup>[2]</sup>**

A binary mask representing only breast parenchyma is extracted

- **Preprocessing**

Image processing techniques are applied with the aim of improving next stages

- **ROI Detection**

Tumour lesions are identified as ROI (Region Of Interest), both malignant and benign

- **ROI Classification**

Each ROI is classified according to its staging

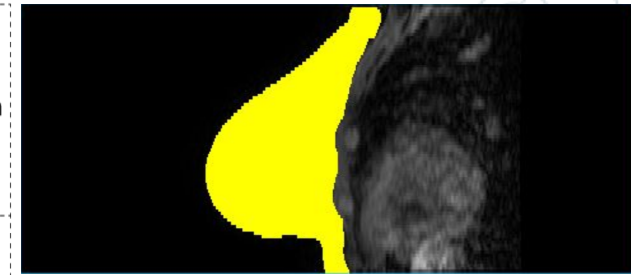
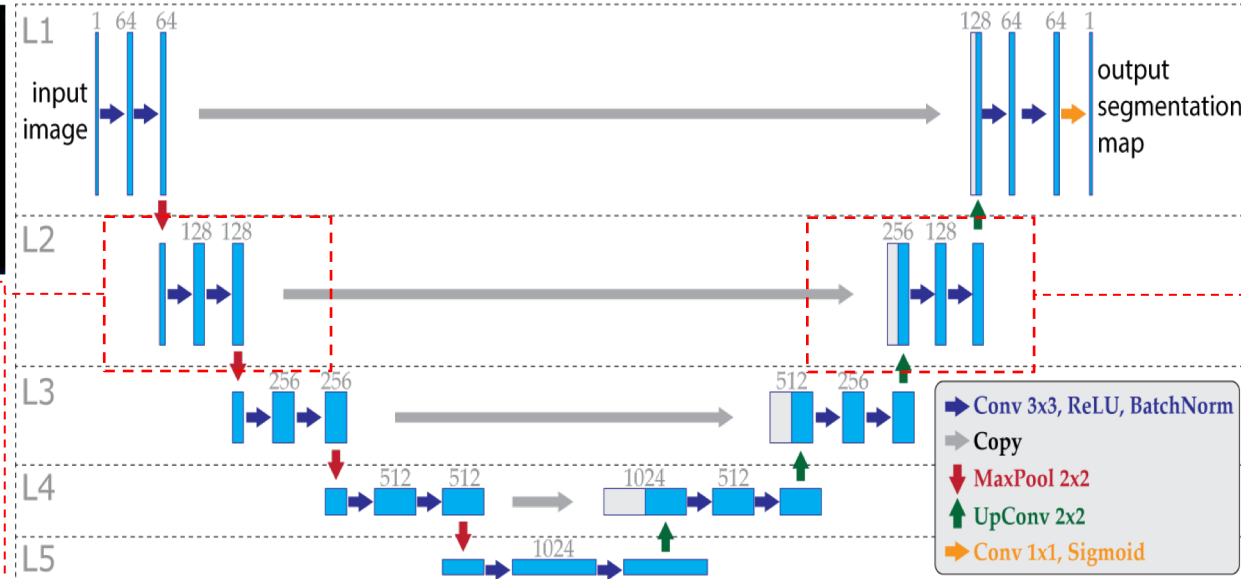
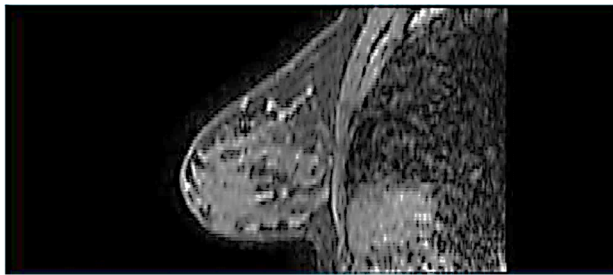


[1]Piantadosi, G., Marrone, S., Fusco, R., Sansone, M., Sansone, C.: A comprehensive computer-aided diagnosis for breast t1w dce-mri via quantitative dynamical features and spatio-temporal local binary patterns. *IET Computer Vision* (August 2018)

[2]Piantadosi, G., Sansone, M., Sansone, C.: Breast Segmentation in MRI via U-Net Deep Convolutional Neural Networks. In: 24rd International Conference on Pattern Recognition (ICPR) (2018)

# Case Study: U-NET for Breast Tissues Segmentation

**U-Shaped networks**<sup>[3]</sup> consist of **two sides** and **several layers**. The left side performs a **contracting path** following the typical architecture of a convolutional neural network. On the other hand, the right side performs the **expansive path** with the same idea of the left side, but aiming to increase the image sizes.



## Contracting path super-layer

1. 2D Conv. (3x3 kernel, zero-padding, stride 1x1)
  2. Rectified Linear Unit (ReLU) activation
  3. Batch Normalisation
  4. 2D Conv. (3x3 kernel, zero-padding, stride 1x1)
  5. Rectified Linear Unit (ReLU) activation
  6. Batch Normalisation
  7. Pooling (max-pool, stride 2x2)
- Performs a down-sampling step halving the size of the image and doubling the size of the feature channels.

**U-Net configuration in ICPR2018**<sup>[2]</sup>: 5 main layers network, 23 convolution layers and 4 max-pooling layers, resulting in a total of 7,771,297 parameters.

[2] Platard, G., Sansone, M., Sansone, C.: Breast Segmentation in MRI via U-Net Deep Convolutional Neural Networks. In: 24th International Conference on Pattern Recognition (ICPR) (2018)

[3] Ronneberger, O., Fischer, P., Brox, T.: U-net: Convolutional networks for biomedical image segmentation. In: International Conference on Medical Image Computing and Computer-Assisted Intervention. pp. 234/241. Springer (2015)

## Expansive path super-layer

1. 2D Up-Conv. (2x2 kernel, zero-padding, stride 1x1)
  2. Concatenation with feature-map from the same level of the contr. path.
  3. 2D Conv. (3x3 kernel, zero-padding, stride 1x1)
  4. Rectified Linear Unit (ReLU) activation
  5. Batch Normalisation
  6. 2D Conv. (3x3 kernel, zero-padding, stride 1x1)
  7. Rectified Linear Unit (ReLU) activation
  8. Batch Normalisation
- The Up-Conv. performs the halving of the feature channels with a trainable kernel.

# Evaluation Strategy

The network was trained by minimizing the task-specific loss:  $1 - \text{DSC}$ . Where DSC is the Dice Similarity Coefficient and  $n(\cdot)$  represents the enclosed volume number of voxels and defined as:

$$\text{DSC} = \frac{2 \cdot n(GS \cap SEG)}{n(GS) + n(SEG)}$$

## Software

Python 3.6  
Keras (front-end)  
TensorFlow 1.9 (back-end)

## Hardware

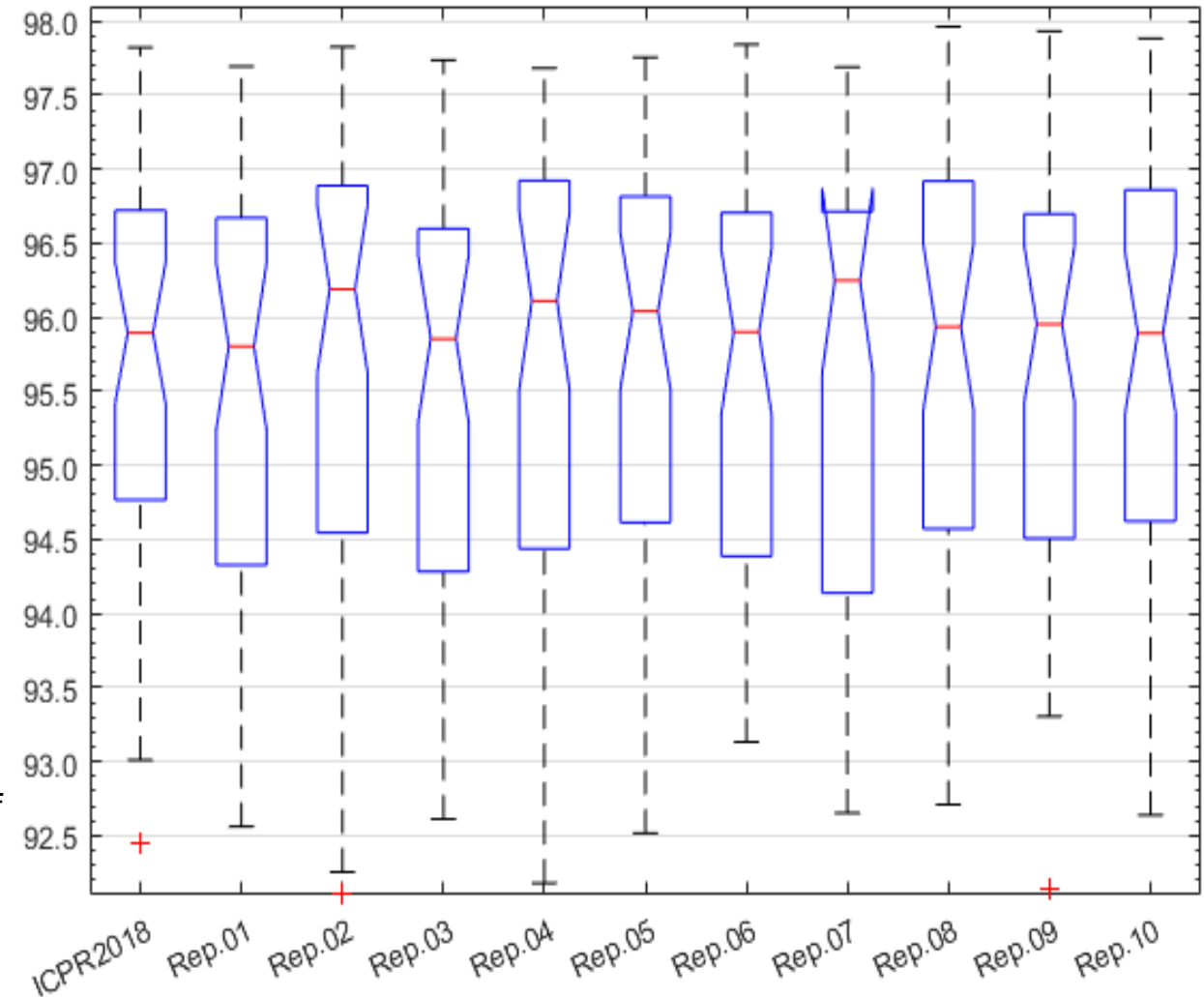
Google Colaboratory (VM)  
2 x Intel(R) Xeon(R) @ 2.2GHz  
CPUs  
13GB RAM  
NVIDIA K80 GPU (12GB GRAM)

- ⊙ Patient-based 10-fold Cross Validation (CV),
- ⊙ Repeatability evaluation: 50 execution with the same initialization seeds for the random numbers generators to try highlighting only the uncertainty due to random considerations introduced by the optimization tools' randomness.

# Results

Repetitions	DSC [%]	LB [%]	UB [%]
<b>ICPR2018<sup>[2]</sup></b>	<b>95.90</b>	<b>95.16</b>	<b>96.64</b>
Rep.01	95.80	95.24	96.37
Rep.02	96.19	95.62	96.75
Rep.03	95.85	95.38	96.39
Rep.04	96.11	95.69	96.57
Rep.05	96.04	95.15	96.62
Rep.06	95.90	95.02	96.60
Rep.07	96.25	95.29	96.52
Rep.08	95.93	95.44	96.56
Rep.09	95.95	95.38	96.36
Rep.10	95.89	95.35	96.43

Results obtained for the first 10 out of 50 Montecarlo executions of the 10-fold cross validation of our approach. The results presented in ICPR2018 are also reported in bold. Median values [left] with corresponding 95% confidence intervals (LB: LowerBound, UB: UpperBound) and boxplots [right] are reported .



# Conclusions

## Key Findings:

- ◎ We quantitatively highlighted the reproducibility problem of Convolutional Neural Networks (CNN) based approaches evaluating our deep learning approach for breast segmentation.
- ◎ We can state that our CNN-based model is stable to the different training executions since the confidence intervals obtained on the tests data overlap.

## General Findings:

- ◎ This problem is not limited to the analyzed framework, Tensorflow, but lies in the NVIDIA CUDA Deep Neural Network (cuDNN) libraries.
- ◎ The randomness introduced with the advent of optimization engines for deep learning models, even if it may impact on the results of a reliable and reproducible research, only shift the attention on the statistical validity of the obtained outcomes.